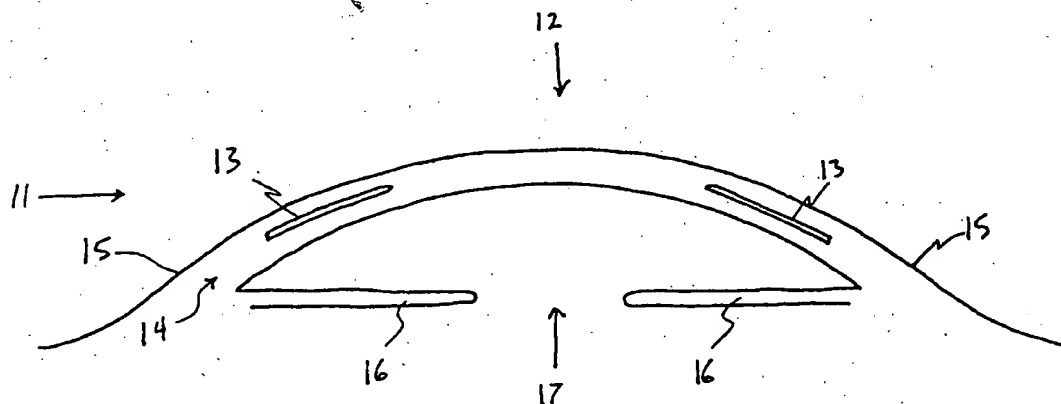




INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶: A61N 5/02	A1	(11) International Publication Number: WO 98/42409 (43) International Publication Date: 1 October 1998 (01.10.98)
(21) International Application Number: PCT/US98/05720 (22) International Filing Date: 24 March 1998 (24.03.98) (30) Priority Data: 08/823,149 25 March 1997 (25.03.97) US (71)(72) Applicant and Inventor: SAWUSCH, Mark, R. [US/US]; 4487 Colbath Avenue #202, Sherman Oaks, CA 91423 (US).		(81) Designated States: AU, BR, JP, MX, SG, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published <i>With international search report.</i> <i>Before the expiration of the time limit for amending the</i> <i>claims and to be republished in the event of the receipt of</i> <i>amendments.</i>

(54) Title: METHOD, IMPLANT, AND APPARATUS FOR REFRACTIVE KERATOPLASTY**(57) Abstract**

A method, implant, and apparatus to alter the refractive power of the cornea. The method involves creation of radial, intrastromal corneal incisions and insertion of semirigid, biocompatible implants (13). An apparatus (26) is provided to facilitate creation of the incisions with precise depth, orientation, and dimension. The implants (13) are of predetermined shape and curvature in accordance with the patient's pre-existing refractive error and corneal curvature. The implants (13) induce a predictable and stable flattening or steepening of corneal curvature for the correction of refractive errors. If residual refractive error is present following this procedure, the curvature or dimensions of the implants may be selectively increased or decreased by application of laser or other energy source to a heat-shrinkable portion of the implants, thereby eliminating residual refractive error.

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece			TR	Turkey
BG	Bulgaria	HU	Hungary	ML	Mali	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MN	Mongolia	UA	Ukraine
BR	Brazil	IL	Israel	MR	Mauritania	UG	Uganda
BY	Belarus	IS	Iceland	MW	Malawi	US	United States of America
CA	Canada	IT	Italy	MX	Mexico	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NE	Niger	VN	Viet Nam
CG	Congo	KE	Kenya	NL	Netherlands	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NO	Norway	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	NZ	New Zealand		
CM	Cameroon			PL	Poland		
CN	China	KR	Republic of Korea	PT	Portugal		
CU	Cuba	KZ	Kazakhstan	RO	Romania		
CZ	Czech Republic	LC	Saint Lucia	RU	Russian Federation		
DE	Germany	LI	Liechtenstein	SD	Sudan		
DK	Denmark	LK	Sri Lanka	SE	Sweden		
EE	Estonia	LR	Liberia	SG	Singapore		

METHOD, IMPLANT, AND APPARATUS FOR REFRACTIVE KERATOPLASTY

BACKGROUND OF THE INVENTION

The invention relates to a method, implant, and apparatus for altering the curvature of the cornea of the eye for the correction of refractive errors.

It is well known that refractive errors can be corrected by reshaping the cornea of the eye to obviate the need for glasses or contact lenses. Reshaping of the cornea may be accomplished in several ways. Prior art techniques of refractive surgery are discussed in detail in the text entitled "Refractive Keratotomy for Myopia and Astigmatism" by George O. Waring III published by Mosby Year Book of St. Louis, MO, 1992. For example, the well known radial keratotomy method for correction of myopia involves the creation of multiple radial incisions through epithelium, Bowman's membrane, and at least 90% of the stromal thickness. This results in marked weakening of the structural integrity of the midperipheral cornea, causing relative steepening in this region and relative flattening of the central corneal curvature. This method has been associated with a number of undesirable factors including undercorrection or overcorrection of refractive error, fluctuating vision, corneal rupture from trauma, regression or progression of refractive effect, inability to correct high myopia, and infection of corneal incisions.

Another method of reshaping the cornea involves the use of lasers to ablate portions of the anterior surface to precise depths, as disclosed in U.S. Pat. No. 4,732,148. This method has also been associated with undercorrection or overcorrection of refractive errors, creation of haze or scarring within the visual axis, regression of refractive effect, a prolonged healing period, and requires use of expensive equipment. U.S. Pat. No. 4,461,294 describes the use of laser energy to vaporize light-absorbing pigments or dyes injected into the corneal stroma to produce multiple radial corneal scars. The corneal scars contract along their length resulting in flattening of central corneal curvature for the correction of myopia. However, variable wound healing following this procedure might result in unpredictable refractive effect.

Intracorneal synthetic or biological implants have been described in the prior art for alteration of corneal curvature. For example, U.S. Pat. No. 4,607,617 describes the implantation of synthetic lenses within the central corneal stroma for correction of refractive errors. These implants and methods have been associated with undesirable side effects including necrosis of tissue anterior to the implant due to interference with nutrient transfer, irreversible scarring and vascularization within the visual axis, undercorrection and overcorrection of refractive error, and the surgery can be technically difficult to perform.

U.S. Pat. No. 5,300,118 and related patents describe the implantation of a single intrastromal, circumferential, biocompatible ring of varied thickness for the correction of refractive errors. This implant exerts a direct conformational change upon the cornea resulting in flattening of the central cornea in proportion to the thickness of the ring. However, this prior art differs from the present invention in several ways, including 1) the present invention utilizes an implant of much smaller dimensions and of a completely different shape, 2) the implants of the present invention are placed radially within the cornea instead of circumferentially, 3) only the present invention allows adjustment of refractive effect by application of heat to the implants, 4) the radial placement of the implants of the present invention is technically easier to perform and is less error-prone than the circumferential placement of the prior art method, 5) the radial placement of the implants of the present invention exert different stress vectors on the cornea than the prior art, 6) the prior art uses one or two ring-shaped implants always placed in the same corneal location whereas the present invention uses 1 to 30 implants placed in a variety of locations, corneal depths, and distances from the central cornea depending on preexisting refractive error, 7) the prior art uses implants all of the same initial curvature whereas the present invention uses implants of various preselected curvatures, 8) the present invention allows more selective alteration of refractive effect by removing and replacing individual small implants which only affects the corneal curvature immediately surrounding the implant instead of large portions of the cornea with the prior art, and 9) the prior art method requires a very different and more complex apparatus to create the corneal incisions for the implant.

U.S. Pat. No. 4,781,187, a modification of the radial keratotomy procedure, describes the suturing of donor corneal tissue implants of rectangular or triangular geometry within conventional radial keratotomy incisions. This method provides variable change in corneal curvature by controlling the amount of gape within radial keratotomy incisions. The implants described in this patent are relatively nonrigid and do not directly exert conformational changes upon the surrounding cornea. These implants maintain the gaping of radial incisions at the corneal surface, thereby increasing the circumference of the mid-peripheral cornea. This prior art differs from the present invention in several ways including the requirement of deep corneal incisions extending to the outer surface of the cornea and is associated with undesirable factors such as difficulty of producing and handling very thin donor corneal implants of precise thickness, and overcorrections or undercorrections due to variable wound healing and variability of suture tightness. The wound healing variability associated with conventional radial keratotomy would also apply to this prior art procedure.

SUMMARY OF THE INVENTION

It is an object of the present invention to overcome the disadvantages associated with prior art techniques of correcting refractive error by modification of corneal curvature.

The present invention provides a means of modifying corneal curvature in a predictable, reversible, and adjustable fashion. The method involves insertion of semirigid, biocompatible implants into the midperipheral corneal stroma. The implants are of predetermined shape and curvature based upon the patient's refractive error and corneal curvature. The implants induce a predictable conformational change in corneal curvature, e.g. central flattening for correction of myopia or steepening for correction of hyperopia. If residual refractive error is present following the initial procedure, the dimensions or curvature of the implants may be altered by the application of heat by laser or other source to a heat-shrinkable portion of the implants. This provides selective enhancement or decrease of refractive effect and may be done at any time following the initial procedure.

It is an object of the invention to alter corneal curvature by inducing conformation of the less rigid cornea to the shape of more rigid implants placed within incisions in the corneal stroma. The creation of intrastromal incisions alone does not result in significant change in corneal curvature (see Sawusch MR, Computer Modeling of Wound Gape Following Radial Keratotomy, Refractive and Corneal Surgery, March/April 1992, p 143-5). The modification of corneal curvature is dependent upon the curvature, corneal location, dimensions, and stiffness or Young's modulus of the corneal implants.

It is another object of the invention to provide an apparatus for the creation of radial, intrastromal corneal incisions of defined depth, length, and diameter to facilitate insertion of the intrastromal implants.

Unlike radial keratotomy (and modifications such as U.S. Patent No. 4,781,187), the present invention does not involve deep incisions through epithelium, Bowman's membrane, and large portions of corneal stroma in order to weaken the structural integrity of the cornea to cause change in shape. Thus, the present invention does not decrease the structural integrity of the cornea. In addition, intrastromal incisions are smaller and would be expected to heal faster and with less scarring and less variability than those required for radial keratotomy. Intrastromal incisions may also be less susceptible to late infection since the corneal epithelium and Bowman's membrane remains largely intact. Preliminary data also suggest that the present invention can effect larger changes in corneal curvature than are possible from radial keratotomy.

It is an object of the invention to alter central corneal curvature secondarily without surgically violating the "central optical zone," the central 3 mm of the corneal apex centered on the visual axis. Unlike excimer laser photorefractive keratectomy or intracorneal lenses, the present invention cannot result in vision-reducing scarring or haze within the central optical zone since this region is not operated upon. In the present invention, the central corneal curvature is altered secondarily by the implants present in the adjacent mid-peripheral cornea. For example, for correction of myopia, the major axis of the implants is relatively more curved than the native cornea and therefore causes a steepening of curvature of the mid-peripheral corneal curvature, which secondarily results in a flattening of the central corneal curvature to correct the refractive error.

It is an object of the invention to provide corneal implants for correction of refractive error which are of sufficiently small transverse diameter so that they do not interfere with nutrient transfer within the cornea and thereby avoid necrosis of corneal tissue.

It is an object of the invention to provide a simple and precise means to modify the effect of surgery at any time following the insertion of the implants. If the patient is left with residual refractive error following the initial procedure and wound healing, the curvature or dimensions of the intrastromal implants may be altered in-situ by the application of laser or other energy source to effect heat-shrinkage of portions of the implants. The laser or other heat source is focused or concentrated on the implant material and may be preferentially absorbed by dyes within the implant material. The adjacent transparent corneal tissue would not absorb the laser energy and therefore no scarring nor wound healing response would result.

It is an object of the invention to allow reversibility of corneal curvature change. If the curvature change is not appropriate or no longer desired, the corneal implants may be removed and the cornea will resume the original shape. The surgeon also has the option of replacing implants with those of a different curvature or dimensions if a different corneal curvature is desired.

These and other objects of the invention will be apparent to those skilled in the art, in light of the accompanying description, drawings and appended claims.

BRIEF DESCRIPTION OF THE FIGURES

Fig 1 is a cross-sectional view of the cornea containing intrastromal implants.

Fig 2 is an isometric view of a suggested shape for an intrastromal implant.

Fig 3 illustrates transverse cross-sectional views of other potential implant shapes.

Fig 4a is an isometric view of a hand-held surgical apparatus used to create radial intrastromal incisions to allow insertion of intrastromal implants.

Fig 4b is a forward end view of the apparatus used to create radial intrastromal incisions.

Fig 5a is an anterior or top view of a cornea containing intrastromal implants in a symmetric pattern of locations.

Fig 5b is an anterior or top view of a cornea containing intrastromal implants in an asymmetric pattern of locations.

Fig 6 is an isometric view of another embodiment of the surgical apparatus used to insert corneal implants.

DESCRIPTION OF PREFERRED EMBODIMENTS

Before explaining the present invention in detail, it is to be understood that the invention is not limited in its application to the details of the construction and arrangement of parts illustrated in the accompanying diagrams. The invention is capable of other embodiments and of being practiced or carried out in a variety of ways. It is to be understood that the phraseology and terminology employed herein is for the purpose of description and not limitation.

The invention is directed at correcting refractive errors of the human or animal eye, including myopia, hyperopia, and astigmatism, by altering the curvature of the cornea. Referring first to Fig 1 of the drawings, a cross-section of the anterior portion of the human eye is shown with the cornea 11 representing the transparent, dome-shaped outer coating of the eye. The central optical zone 12 is the portion of the cornea which corresponds to the visual axis. In patients having myopia, the central corneal curvature is too steep and the light rays are focused in front of the retina; flattening of the cornea allows light rays to focus on the retina for clear vision. In patients having hyperopia, the central corneal curvature is too flat and the light rays are focused behind the retina; steepening of the cornea allows light rays to focus on the retina. Placement of semirigid radial implants 13 having selected curvature or dimensions within the corneal stroma 14 results in a predictable steepening or flattening of the central cornea to correct refractive errors. Fig 1 also illustrates additional anatomic features of the eye including the peripheral aspect of the cornea called the limbus 15, the iris 16, and the pupil 17.

The surgeon must first determine the patient's refractive error and corneal curvature by conventional means, including use of a keratometer or corneal topography mapping device. Refraction, keratometry, and patient age variables are employed by a nomogram or computer program to select the curvature, dimensions, and number of implants, and locations within the cornea of each implant necessary to achieve a desired refractive effect. Locations within the cornea may be specified in three dimensions, i.e. the meridian in degrees, the relative corneal depth, and the proximity to the center of the cornea. Finite

element modeling or empirical data may be used to assist in determining these variables for a given cornea.

The corneal implant curvature and dimensions have been selected according to the nomogram or computer program as described above. Fig 2 illustrates one embodiment of the shape of the corneal implants. The leading end or tip 20 of the implant may be rounded, flat, or tapered to facilitate dissection of tissue during insertion. Fig 3 illustrates transverse cross-sectional views of other embodiments of the shape of the corneal implants. The cross-sectional dimensions may be held constant throughout the length of the implant or progressively diminished to allow a more pointed configuration. The implants are available in a variety of lengths, transverse shapes, and curvatures along the longitudinal axis to allow for the correction of a wide variety of refractive errors. For example, implants that have a greater curvature than a given cornea may result in central corneal flattening to correct myopia, whereas implants that have a lesser or inverse curvature than a given cornea may result in central corneal steepening to correct hyperopia. Implants which are longer or of wider transverse dimensions would also tend to produce a greater change in corneal curvature. Implants placed within one meridian may add cylindrical power if more curved than the cornea in that meridian or subtract cylindrical power if less curved than the cornea in that meridian. The implants may be fashioned from semi-rigid biocompatible materials including, but not limited to, polymethylmethacrylate (PMMA), Prolene (TM), Sauflon (TM), acrylic, nylon (TM), and other heat-shrinkable plastics. Dyes may be incorporated within the implant material to increase the absorption of light energy from a laser or other heat source. The dye may be present throughout the entire implant or limited to particular portions of the implant.

The procedure may be performed in the following fashion. The cornea is anesthetized with topical anesthetic drops. The optical center of the cornea is marked while the patient stares at a fixation light. An optical zone marker is centered over the optical center and radial keratotomy incision marker used to assist in orienting intrastromal incisions. These steps are identical to those prior to performing radial keratotomy and are described in detail in the above reference by Waring. A guarded surgical blade is placed at the peripheral aspect of each incision mark and used to make a small radial incision to a depth of approximately 400-500 microns or approximately one-half peripheral corneal thickness.

The apparatus shown in Fig 4a may be used to create radial, intrastromal incisions of desired depth and dimension. The apparatus is preferably formed from stainless steel or titanium. The apparatus consists of two handles 22 tapered and joined at one end by a spring 23. At the other end the handles are joined by a pivot 24 allowing the handles to be squeezed together. The extension of one of the handles beyond the pivot consists of an angled portion 26 that is narrow, elongated, and tapered to permit penetration and dissection of corneal tissue. The extension beyond the pivot of the other handle consists of a angled and widened member, the footplate 28, which may be placed on the corneal surface and used to maintain the position of the apparatus while the handles are squeezed together. The stromal dissector 26 is displaced from the footplate 28 at the desired depth for the corneal implants below the corneal surface. This device is placed with the footplate 28 adjacent to the previously made peripheral corneal incision and oriented in alignment with the radial incision mark. The spring handles 22 are then squeezed by the surgeon to dissect within the corneal lamellae and create a radial intrastromal incision with a diameter the same as that of the stromal dissector 26. Once the stromal dissector 26 has reached the optical zone mark,

the pressure on the spring handles 22 is released to allow the spring handles 23 to remove the stromal dissector 26 from the cornea. This process is repeated in other corneal meridians to create the desired number of intrastromal incisions called for by the nomogram or computer program. Alternatively, the surgeon may use a freehand hypodermic or solid needle or thin blade to create the radial intrastromal incisions. Alternatively, the corneal implant may be injected into virgin corneal tissue to create an incision simultaneous with placement of the implant. With each of these methods, the intrastromal incisions remain within the corneal stroma throughout their length and do not violate Bowman's membrane or epithelium anteriorly (except at the initial entry point of the incision) nor violate Descemet's membrane posteriorly.

The corneal implant curvature and dimension have been selected according to the nomogram or computer program as described above. The surgeon then inserts or injects the corneal implant into the intrastromal incision all the way to the optical zone mark. It may be necessary to push down on the cornea just anterior to the implant as it is inserted to assist in free passage. The entire implant will rest within the incision such that no portion is exposed. If necessary, a suture may be used to close the initial peripheral incision if gaping occurs. This process is repeated until the desired number of implants have been placed. Fig 5a illustrates an anterior or top view of a cornea containing four radial stromal implants 30. Note that the implants are present within the midperipheral cornea and do not enter the central optical zone or "visual axis," the area immediately surrounding the center of the cornea or corneal apex 32. Note placement of the implants radially with respect to the corneal apex 32 and the corneal periphery or limbus 34. Although this Figure illustrates a symmetric placement of implants, an asymmetric placement may be indicated for correction of astigmatism. One example of this is shown in Fig 5b. In addition, the number of implants to be used may range between 1 to 30, depending upon the type and degree of refractive error to be corrected.

Postoperatively, if residual refractive error is present and it is desirable to correct it, a laser or other heat source can be focused or directed upon the implants within the corneal stroma to effect a change in the implant curvature or dimensions due to heat-shrinkage of the implant material. A suitable laser source would be a typical ophthalmic Argon laser which can be focused to a 50-100 μm spot size and applied accurately to a small portion of the intrastromal implant material. The 488nm or 514nm wavelength of the Argon laser is not absorbed by transparent corneal tissue, but can be selectively absorbed by dyes within the implant material. The amount of change of the curvature or dimensions may be precisely controlled by altering the number of laser applications, the location of laser applications, dye concentration or composition within the implant, the energy per application, the laser spot size, and the laser wavelength. The curvature or length change desired for each intrastromal implant can be determined based upon the corneal curvature immediately surrounding each implant, as can be determined by computerized corneal topography or keratometry. Since heat-shrinkage of the implant material is likely to reduce the conformational change exerted by the implant, it may be desirable to select an initial implant curvature or dimensions which are likely to over-correct the refractive error and then use the laser to accurately reduce the over-correction until the corneal curvature provides the desired refractive error or emmetropia.

Should the implants ever require removal, such as due to selection of incorrect implant dimensions or curvature, a small radial incision may be made in the corneal periphery over the implant material in the

same fashion as described above. The implant material may then be withdrawn with a forceps and the intrastromal incision left empty or a new implant placed within the incision as described above. If the implant material is removed and not replaced, it is expected that the corneal shape and refractive change will be reversible and return to the preoperative state.

Fig 6 illustrates a second embodiment of the apparatus used to facilitate insertion of the intrastromal implants. This embodiment permits simultaneous creation of intrastromal incisions and insertion of intrastromal implants. The apparatus consists of an adapted hypodermic syringe with a narrow tube 40 fitted at one end with a piston 42 and at the other end with a hollow needle 43 and hub assembly 47. An advancing wire 45 extends between the piston 42 and the needle 43. The corneal implant is placed entirely within the bore of the needle 43 between the forward cutting end of the needle and the forward end of the advancing wire 45. This apparatus does not require creation of a separate initial peripheral radial incision. The needle 43 may be curved to facilitate orientation of the needle in the radial direction from corneal periphery to the corneal apex while the syringe 40 is held approximately perpendicular to the corneal limbus. The implant material is preloaded into the bore of the needle in the proper orientation, e.g. curvature up or down. Corneal optical zone markers are used to create marks at the entrance site of the needle in the corneal periphery and at the central optical zone. Radial marks may be made with a conventional radial keratotomy corneal marker to connect the peripheral and central marks. The apparatus is placed with a portion of the needle 43 firmly in contact with the peripheral cornea, limbus, and sclera. The needle 43 is also oriented radially with respect to the center of the cornea and such that the tip enters the cornea at the peripheral corneal mark. The forward cutting end of the needle 43 is then advanced toward the central cornea by the surgeon until reaching the central optical zone mark. The portion of the needle 43 that has not yet entered the corneal stroma remains in contact with the surface of the cornea, limbus, and sclera while the needle 43 is advanced. This serves to stabilize and orient the needle so that it travels within the corneal stroma. The advancing wire 45 is then advanced into the bore of the needle 43 by pushing on the piston 42 in order to push the implant material out of the needle 43 and into the corneal stroma. Advancement of the piston is facilitated by countertraction on the syringe flange 48. Simultaneously, the surgeon removes the needle 43 from the corneal stroma while the implant material is advanced into the stroma, thereby allowing the implant to occupy the potential space created by the needle 43. This allows placement of the implant material within the corneal stroma while minimizing disturbance of surrounding tissue. Alternatively, the implant may be fashioned with a sharpened tip to permit dissection of corneal stroma by advancement of the implant rather than by the needle 43.

While particular embodiments of the invention have been shown and described, it will be obvious to those skilled in the art that changes and modifications may be made without departing from the invention in its broader aspects.

I claim:

1. A method for altering corneal curvature to correct refractive errors, including the steps of:
 - determining pre-existing corneal curvature and refractive error,
 - use of a nomogram or computer program encompassing these variables to determine the required locations, number, depth, and dimensions of corneal implants to correct the refractive error,
 - use of an apparatus to create radial, intrastromal corneal incisions of desired depth and dimensions,
 - insertion of biocompatible implants within said incisions to exert conformational change upon corneal curvature,
 - later modification of the dimensions or curvature of said implants by application of heat from a laser or other means, if required to correct residual refractive error,
 - later modification of dimensions or placement of said implants by removal of implants and replacement by other implants of differing dimensions, if required to correct residual refractive error.
2. The method of claim 1, wherein said incisions are made from the corneal periphery or limbus and extend radially toward the central cornea but do not enter the central visual axis of the cornea.
3. The method of claim 1, wherein said incisions remain within the stroma of the cornea except for the initial entrance at the surface of the cornea.
4. The method of claim 1, wherein said incisions may be created in a two step process whereby a small radial incision is made in the corneal periphery or limbus, followed by a radial incision that begins and continues entirely within the corneal stroma.
5. The method of claim 1, wherein said incisions may be single or a plurality of radial incisions placed symmetrically or asymmetrically to correct particular refractive errors.
6. The method of claim 1, wherein the conformational change exerted upon the cornea from said implants may be changed in-situ by altering the longitudinal or transverse dimensions or curvature of said implants by application of heat from a laser or other source to said implants.
7. The method of claim 1, wherein the conformational change exerted upon the cornea from said implants may be reversed by removal of said implants.
8. The method of claim 1, wherein the conformational change exerted upon the cornea by said implants may be altered by removal of said implants and replacement with said implants of different dimensions.
9. A corneal implant, comprising an elongated body of biocompatible material and curved along the longitudinal dimension.

10. The implant of claim 9, wherein said body of material is composed of polymethylmethacrylate.
11. The implant of claim 9, wherein said body of material is composed of prolene (TM).
12. The implant of claim 9, wherein the longitudinal dimensions may be tapered to facilitate dissection of corneal tissue during insertion.
13. The method of claim 1, wherein said incisions are made by advancing an implant of claim 12 within the corneal stroma.
14. The implant of claim 9, wherein the transverse dimensions may be a plurality of shapes.
15. The implant of claim 9, wherein said body of material is composed of heat-shrinkable plastic.
16. The implant of claim 9, wherein dyes are incorporated within said body of material to allow increased absorption of laser or heat energy by said implant.
17. An apparatus for creation of radial intrastromal incisions extending from the corneal periphery or limbus toward the central cornea, comprising:
 - two handles joined at one end by a spring and at the other end pivoted together
 - a forward end of one of said handles consisting of an angled, narrow, elongated, and tapered member for use in penetrating the corneal surface and dissecting corneal stroma
 - a forward end of the other of said handles consisting of an angled member of sufficient width and length to stabilize said apparatus when placed upon the cornea.
18. An apparatus for creation of radial intrastromal incisions and simultaneous insertion of corneal implants comprising:
 - a syringe consisting of a narrow tube fitted at one end with a piston and at the other end by a hollow needle
 - an advancing wire extending from said piston into said needle
 - an implant of claim 9 present within the bore of said needle between the tip of said needle and said advancing wire within said needle.
19. The apparatus of claim 18, wherein the needle of said apparatus is curved to facilitate insertion and advancement of said needle within the corneal stroma from the corneal periphery or limbus toward the corneal apex.

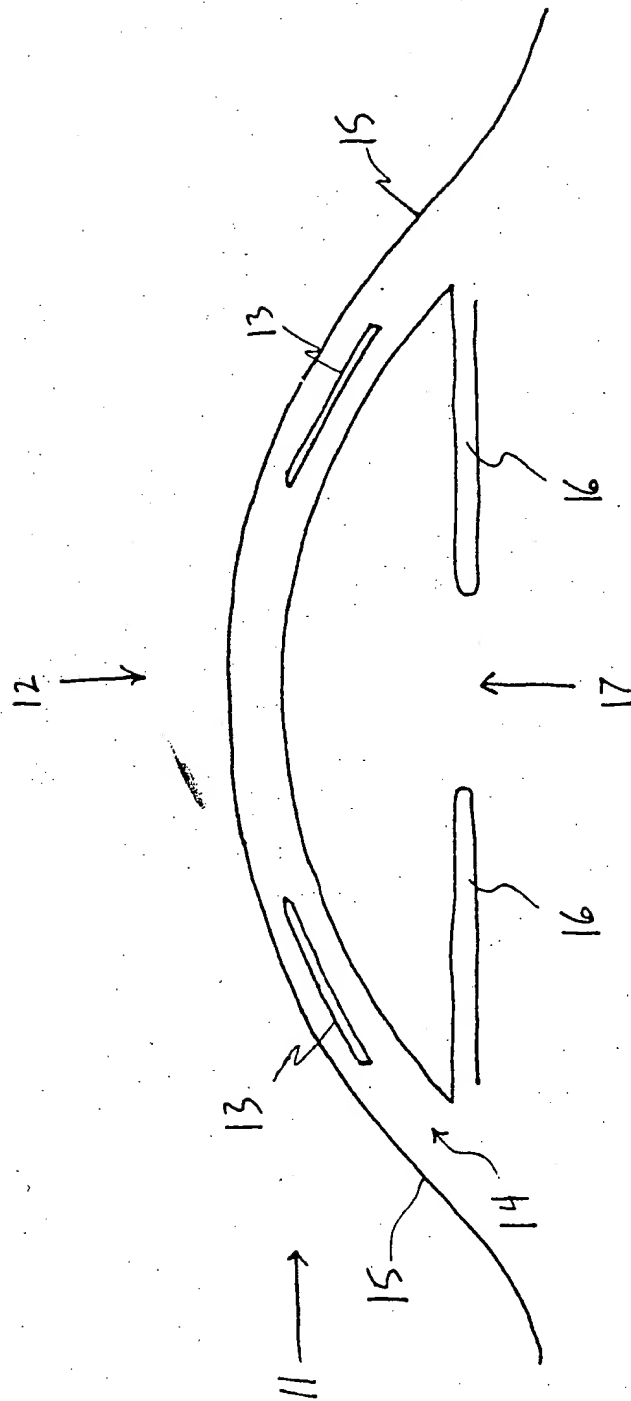


Fig. 1



Fig. 2

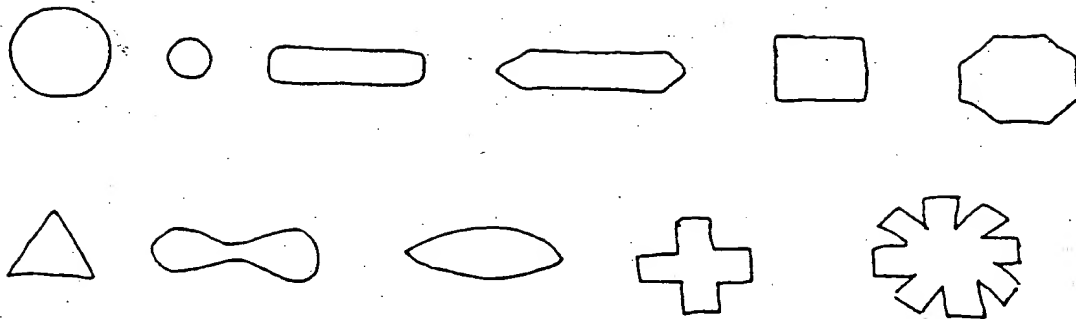


Fig. 3

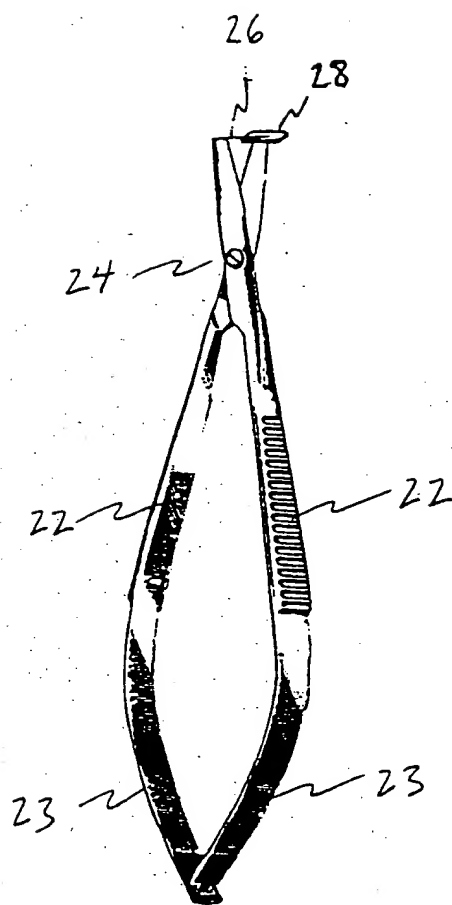
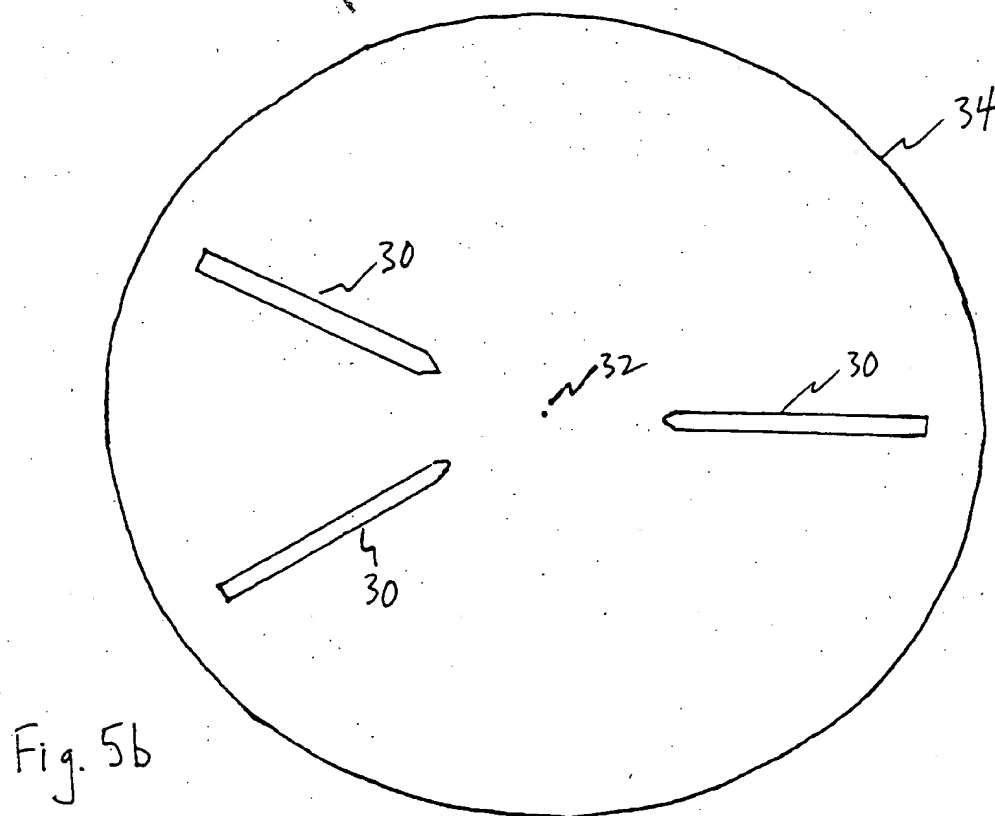
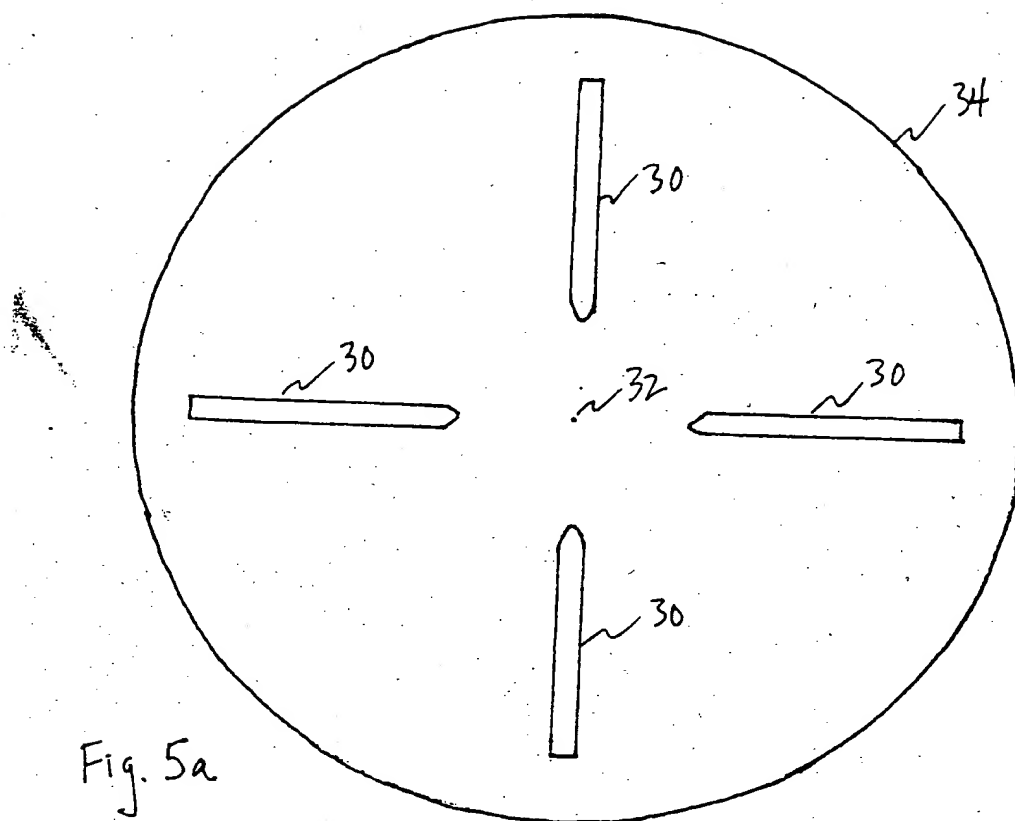


Fig. 4a



Fig. 4b



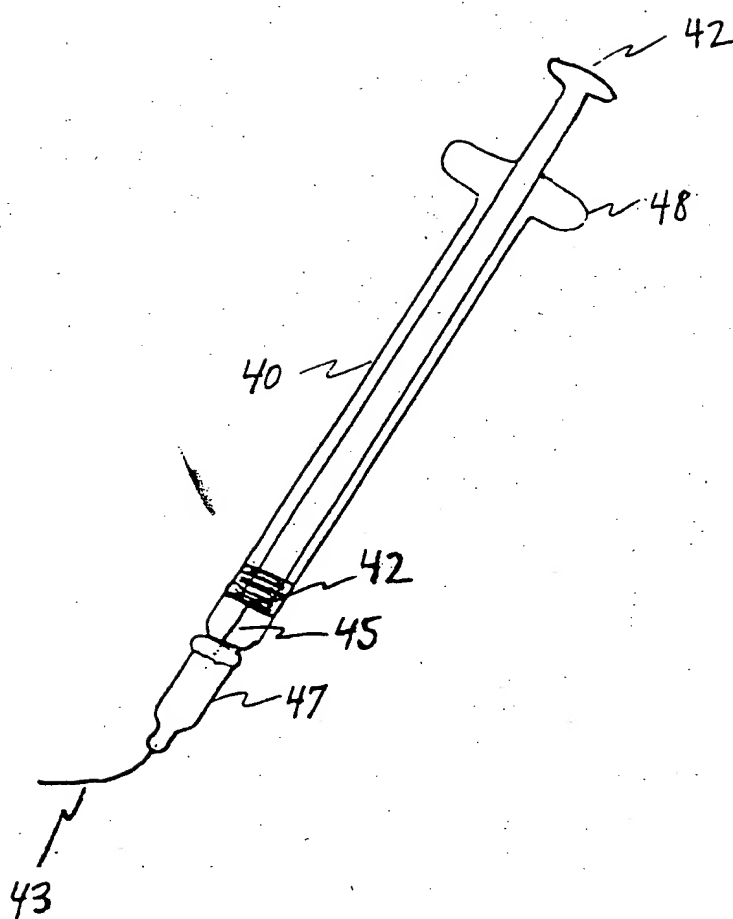


Fig. 6

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US98/05720

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) : A61N 5-02

US CL : 606/5: 128-898

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 606/5: 128/898

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y, P	US 5, 722, 971 A (PEYMAN) 03 MARCH 1998, SEE ENTIRE DOCUMENT	1-19
A	US 5, 425, 727 A (KOZIOL) 20 JUNE 1995, SEE ENTIRE DOCUMENT	1-19

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents	* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
* A* document defining the general state of the art which is not considered to be of particular relevance	* X* document of particular relevance, the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
* E* earlier document published on or after the international filing date	* Y* document of particular relevance, the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
* I* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	* &* document member of the same patent family
* O* document referring to an oral disclosure, use, exhibition or other means	
* P* document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

05 JULY 1998

Date of mailing of the international search report

23 JUL 1998

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
Box PCT
Washington, D.C. 20231

Facsimile No. (703) 305-3230

Authorized officer

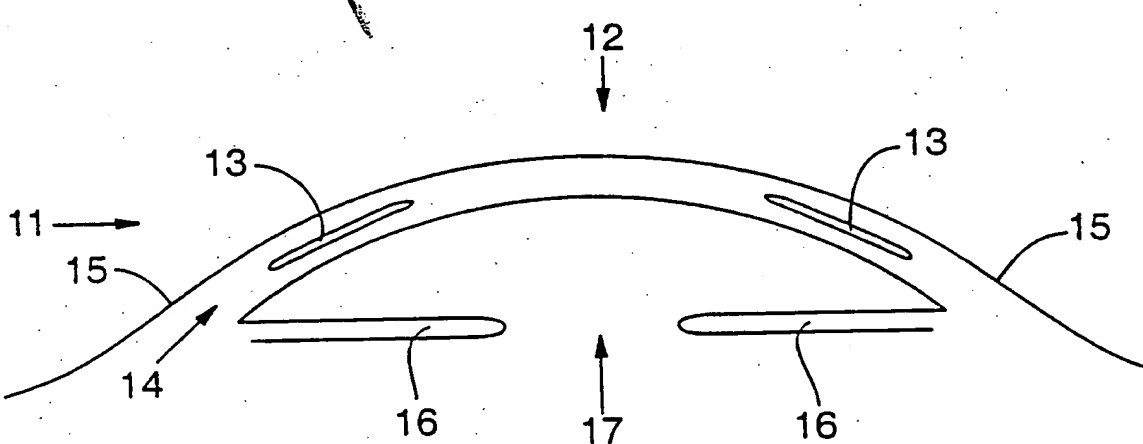
DAVID J. ISABELLA

Telephone No. (703) 308-3060

This Page Blank (uspto)



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶ : A61N 5/02	A1	(11) International Publication Number: WO 98/42409 (43) International Publication Date: 1 October 1998 (01.10.98)
(21) International Application Number: PCT/US98/05720 (22) International Filing Date: 24 March 1998 (24.03.98) (30) Priority Data: 08/823,149 25 March 1997 (25.03.97) US (71)(72) Applicant and Inventor: SAWUSCH, Mark, R. [US/US]; 4487 Colbath Avenue #202, Sherman Oaks, CA 91423 (US).		(81) Designated States: AU, BR, JP, MX, SG, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>
<p>(54) Title: METHOD, IMPLANT, AND APPARATUS FOR REFRACTIVE KERATOPLASTY</p>  <p>(57) Abstract</p> <p>A method, implant, and apparatus to alter the refractive power of the cornea. The method involves creation of radial, intrastromal corneal incisions and insertion of semirigid, biocompatible implants (13). An apparatus (26) is provided to facilitate creation of the incisions with precise depth, orientation, and dimension. The implants (13) are of predetermined shape and curvature in accordance with the patient's pre-existing refractive error and corneal curvature. The implants (13) induce a predictable and stable flattening or steepening of corneal curvature for the correction of refractive errors. If residual refractive error is present following this procedure, the curvature or dimensions of the implants may be selectively increased or decreased by application of laser or other energy source to a heat-shrinkable portion of the implants, thereby eliminating residual refractive error.</p>		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

METHOD, IMPLANT, AND APPARATUS FOR REFRACTIVE KERATOPLASTY

BACKGROUND OF THE INVENTION

The invention relates to a method, implant, and apparatus for altering the curvature of the cornea of the eye for the correction of refractive errors.

It is well known that refractive errors can be corrected by reshaping the cornea of the eye to obviate the need for glasses or contact lenses. Reshaping of the cornea may be accomplished in several ways. Prior art techniques of refractive surgery are discussed in detail in the text entitled "Refractive Keratotomy for Myopia and Astigmatism" by George O. Waring III published by Mosby Year Book of St. Louis, MO, 1992. For example, the well known radial keratotomy method for correction of myopia involves the creation of multiple radial incisions through epithelium, Bowman's membrane, and at least 90% of the stromal thickness. This results in marked weakening of the structural integrity of the midperipheral cornea, causing relative steepening in this region and relative flattening of the central corneal curvature. This method has been associated with a number of undesirable factors including undercorrection or overcorrection of refractive error, fluctuating vision, corneal rupture from trauma, regression or progression of refractive effect, inability to correct high myopia, and infection of corneal incisions.

Another method of reshaping the cornea involves the use of lasers to ablate portions of the anterior surface to precise depths, as disclosed in U.S. Pat. No. 4,732,148. This method has also been associated with undercorrection or overcorrection of refractive errors, creation of haze or scarring within the visual axis, regression of refractive effect, a prolonged healing period, and requires use of expensive equipment. U.S. Pat. No. 4,461,294 describes the use of laser energy to vaporize light-absorbing pigments or dyes injected into the corneal stroma to produce multiple radial corneal scars. The corneal scars contract along their length resulting in flattening of central corneal curvature for the correction of myopia. However, variable wound healing following this procedure might result in unpredictable refractive effect.

Intracorneal synthetic or biological implants have been described in the prior art for alteration of corneal curvature. For example, U.S. Pat. No. 4,607,617 describes the implantation of synthetic lenses within the central corneal stroma for correction of refractive errors. These implants and methods have been associated with undesirable side effects including necrosis of tissue anterior to the implant due to interference with nutrient transfer, irreversible scarring and vascularization within the visual axis, undercorrection and overcorrection of refractive error, and the surgery can be technically difficult to perform.

U.S. Pat. No. 5,300,118 and related patents describe the implantation of a single intrastromal, circumferential, biocompatible ring of varied thickness for the correction of refractive errors. This implant exerts a direct conformational change upon the cornea resulting in flattening of the central cornea in proportion to the thickness of the ring. However, this prior art differs from the present invention in several ways, including 1) the present invention utilizes an implant of much smaller dimensions and of a completely different shape, 2) the implants of the present invention are placed radially within the cornea instead of circumferentially, 3) only the present invention allows adjustment of refractive effect by application of heat to the implants, 4) the radial placement of the implants of the present invention is technically easier to perform and is less error-prone than the circumferential placement of the prior art method, 5) the radial placement of the implants of the present invention exert different stress vectors on the cornea than the prior art, 6) the prior art uses one or two ring-shaped implants always placed in the same corneal location whereas the present invention uses 1 to 30 implants placed in a variety of locations, corneal depths, and distances from the central cornea depending on preexisting refractive error, 7) the prior art uses implants all of the same initial curvature whereas the present invention uses implants of various preselected curvatures, 8) the present invention allows more selective alteration of refractive effect by removing and replacing individual small implants which only affects the corneal curvature immediately surrounding the implant instead of large portions of the cornea with the prior art, and 9) the prior art method requires a very different and more complex apparatus to create the corneal incisions for the implant.

U.S. Pat. No. 4,781,187, a modification of the radial keratotomy procedure, describes the suturing of donor corneal tissue implants of rectangular or triangular geometry within conventional radial keratotomy incisions. This method provides variable change in corneal curvature by controlling the amount of gape within radial keratotomy incisions. The implants described in this patent are relatively nonrigid and do not directly exert conformational changes upon the surrounding cornea. These implants maintain the gaping of radial incisions at the corneal surface, thereby increasing the circumference of the mid-peripheral cornea. This prior art differs from the present invention in several ways including the requirement of deep corneal incisions extending to the outer surface of the cornea and is associated with undesirable factors such as difficulty of producing and handling very thin donor corneal implants of precise thickness, and overcorrections or undercorrections due to variable wound healing and variability of suture tightness. The wound healing variability associated with conventional radial keratotomy would also apply to this prior art procedure.

SUMMARY OF THE INVENTION

It is an object of the present invention to overcome the disadvantages associated with prior art techniques of correcting refractive error by modification of corneal curvature.

The present invention provides a means of modifying corneal curvature in a predictable, reversible, and adjustable fashion. The method involves insertion of semirigid, biocompatible implants into the midperipheral corneal stroma. The implants are of predetermined shape and curvature based upon the patient's refractive error and corneal curvature. The implants induce a predictable conformational change in corneal curvature, e.g. central flattening for correction of myopia or steepening for correction of hyperopia. If residual refractive error is present following the initial procedure, the dimensions or curvature of the implants may be altered by the application of heat by laser or other source to a heat-shrinkable portion of the implants. This provides selective enhancement or decrease of refractive effect and may be done at any time following the initial procedure.

It is an object of the invention to alter corneal curvature by inducing conformation of the less rigid cornea to the shape of more rigid implants placed within incisions in the corneal stroma. The creation of intrastromal incisions alone does not result in significant change in corneal curvature (see Sawusch MR, Computer Modeling of Wound Gape Following Radial Keratotomy, Refractive and Corneal Surgery, March/April 1992, p 143-5). The modification of corneal curvature is dependent upon the curvature, corneal location, dimensions, and stiffness or Young's modulus of the corneal implants.

It is another object of the invention to provide an apparatus for the creation of radial, intrastromal corneal incisions of defined depth, length, and diameter to facilitate insertion of the intrastromal implants.

Unlike radial keratotomy (and modifications such as U.S. Patent No. 4,781,187), the present invention does not involve deep incisions through epithelium, Bowman's membrane, and large portions of corneal stroma in order to weaken the structural integrity of the cornea to cause change in shape. Thus, the present invention does not decrease the structural integrity of the cornea. In addition, intrastromal incisions are smaller and would be expected to heal faster and with less scarring and less variability than those required for radial keratotomy. Intrastromal incisions may also be less susceptible to late infection since the corneal epithelium and Bowman's membrane remains largely intact. Preliminary data also suggest that the present invention can effect larger changes in corneal curvature than are possible from radial keratotomy.

It is an object of the invention to alter central corneal curvature secondarily without surgically violating the "central optical zone," the central 3 mm of the corneal apex centered on the visual axis. Unlike excimer laser photorefractive keratectomy or intracorneal lenses, the present invention cannot result in vision-reducing scarring or haze within the central optical zone since this region is not operated upon. In the present invention, the central corneal curvature is altered secondarily by the implants present in the adjacent mid-peripheral cornea. For example, for correction of myopia, the major axis of the implants is relatively more curved than the native cornea and therefore causes a steepening of curvature of the mid-peripheral corneal curvature, which secondarily results in a flattening of the central corneal curvature to correct the refractive error.

It is an object of the invention to provide corneal implants for correction of refractive error which are of sufficiently small transverse diameter so that they do not interfere with nutrient transfer within the cornea and thereby avoid necrosis of corneal tissue.

It is an object of the invention to provide a simple and precise means to modify the effect of surgery at any time following the insertion of the implants. If the patient is left with residual refractive error following the initial procedure and wound healing, the curvature or dimensions of the intrastromal implants may be altered in-situ by the application of laser or other energy source to effect heat-shrinkage of portions of the implants. The laser or other heat source is focused or concentrated on the implant material and may be preferentially absorbed by dyes within the implant material. The adjacent transparent corneal tissue would not absorb the laser energy and therefore no scarring nor wound healing response would result.

It is an object of the invention to allow reversibility of corneal curvature change. If the curvature change is not appropriate or no longer desired, the corneal implants may be removed and the cornea will resume the original shape. The surgeon also has the option of replacing implants with those of a different curvature or dimensions if a different corneal curvature is desired.

These and other objects of the invention will be apparent to those skilled in the art, in light of the accompanying description, drawings and appended claims.

BRIEF DESCRIPTION OF THE FIGURES

Fig 1 is a cross-sectional view of the cornea containing intrastromal implants.

Fig 2 is an isometric view of a suggested shape for an intrastromal implant.

Fig 3 illustrates transverse cross-sectional views of other potential implant shapes.

Fig 4a is an isometric view of a hand-held surgical apparatus used to create radial intrastromal incisions to allow insertion of intrastromal implants.

Fig 4b is a forward end view of the apparatus used to create radial intrastromal incisions.

Fig 5a is an anterior or top view of a cornea containing intrastromal implants in a symmetric pattern of locations.

Fig 5b is an anterior or top view of a cornea containing intrastromal implants in an asymmetric pattern of locations.

Fig 6 is an isometric view of another embodiment of the surgical apparatus used to insert corneal implants.

DESCRIPTION OF PREFERRED EMBODIMENTS

Before explaining the present invention in detail, it is to be understood that the invention is not limited in its application to the details of the construction and arrangement of parts illustrated in the accompanying diagrams. The invention is capable of other embodiments and of being practiced or carried out in a variety of ways. It is to be understood that the phraseology and terminology employed herein is for the purpose of description and not limitation.

The invention is directed at correcting refractive errors of the human or animal eye, including myopia, hyperopia, and astigmatism, by altering the curvature of the cornea. Referring first to Fig 1 of the drawings, a cross-section of the anterior portion of the human eye is shown with the cornea 11 representing the transparent, dome-shaped outer coating of the eye. The central optical zone 12 is the portion of the cornea which corresponds to the visual axis. In patients having myopia, the central corneal curvature is too steep and the light rays are focused in front of the retina; flattening of the cornea allows light rays to focus on the retina for clear vision. In patients having hyperopia, the central corneal curvature is too flat and the light rays are focused behind the retina; steepening of the cornea allows light rays to focus on the retina. Placement of semirigid radial implants 13 having selected curvature or dimensions within the corneal stroma 14 results in a predictable steepening or flattening of the central cornea to correct refractive errors. Fig 1 also illustrates additional anatomic features of the eye including the peripheral aspect of the cornea called the limbus 15, the iris 16, and the pupil 17.

The surgeon must first determine the patient's refractive error and corneal curvature by conventional means, including use of a keratometer or corneal topography mapping device. Refraction, keratometry, and patient age variables are employed by a nomogram or computer program to select the curvature, dimensions, and number of implants, and locations within the cornea of each implant necessary to achieve a desired refractive effect. Locations within the cornea may be specified in three dimensions, i.e. the meridian in degrees, the relative corneal depth, and the proximity to the center of the cornea. Finite

element modeling or empirical data may be used to assist in determining these variables for a given cornea.

The corneal implant curvature and dimensions have been selected according to the nomogram or computer program as described above. Fig 2 illustrates one embodiment of the shape of the corneal implants. The leading end or tip 20 of the implant may be rounded, flat, or tapered to facilitate dissection of tissue during insertion. Fig 3 illustrates transverse cross-sectional views of other embodiments of the shape of the corneal implants. The cross-sectional dimensions may be held constant throughout the length of the implant or progressively diminished to allow a more pointed configuration. The implants are available in a variety of lengths, transverse shapes, and curvatures along the longitudinal axis to allow for the correction of a wide variety of refractive errors. For example, implants that have a greater curvature than a given cornea may result in central corneal flattening to correct myopia, whereas implants that have a lesser or inverse curvature than a given cornea may result in central corneal steepening to correct hyperopia. Implants which are longer or of wider transverse dimensions would also tend to produce a greater change in corneal curvature. Implants placed within one meridian may add cylindrical power if more curved than the cornea in that meridian or subtract cylindrical power if less curved than the cornea in that meridian. The implants may be fashioned from semi-rigid biocompatible materials including, but not limited to, polymethylmethacrylate (PMMA), Prolene (TM), Sauflon (TM), acrylic, nylon (TM), and other heat-shrinkable plastics. Dyes may be incorporated within the implant material to increase the absorption of light energy from a laser or other heat source. The dye may be present throughout the entire implant or limited to particular portions of the implant.

The procedure may be performed in the following fashion. The cornea is anesthetized with topical anesthetic drops. The optical center of the cornea is marked while the patient stares at a fixation light. An optical zone marker is centered over the optical center and radial keratotomy incision marker used to assist in orienting intrastromal incisions. These steps are identical to those prior to performing radial keratotomy and are described in detail in the above reference by Waring. A guarded surgical blade is placed at the peripheral aspect of each incision mark and used to make a small radial incision to a depth of approximately 400-500 microns or approximately one-half peripheral corneal thickness.

The apparatus shown in Fig 4a may be used to create radial, intrastromal incisions of desired depth and dimension. The apparatus is preferably formed from stainless steel or titanium. The apparatus consists of two handles 22 tapered and joined at one end by a spring 23. At the other end the handles are joined by a pivot 24 allowing the handles to be squeezed together. The extension of one of the handles beyond the pivot consists of an angled portion 26 that is narrow, elongated, and tapered to permit penetration and dissection of corneal tissue. The extension beyond the pivot of the other handle consists of a angled and widened member, the footplate 28, which may be placed on the corneal surface and used to maintain the position of the apparatus while the handles are squeezed together. The stromal dissector 26 is displaced from the footplate 28 at the desired depth for the corneal implants below the corneal surface. This device is placed with the footplate 28 adjacent to the previously made peripheral corneal incision and oriented in alignment with the radial incision mark. The spring handles 22 are then squeezed by the surgeon to dissect within the corneal lamellae and create a radial intrastromal incision with a diameter the same as that of the stromal dissector 26. Once the stromal dissector 26 has reached the optical zone mark,

the pressure on the spring handles 22 is released to allow the spring handles 23 to remove the stromal dissector 26 from the cornea. This process is repeated in other corneal meridians to create the desired number of intrastromal incisions called for by the nomogram or computer program. Alternatively, the surgeon may use a freehand hypodermic or solid needle or thin blade to create the radial intrastromal incisions. Alternatively, the corneal implant may be injected into virgin corneal tissue to create an incision simultaneous with placement of the implant. With each of these methods, the intrastromal incisions remain within the corneal stroma throughout their length and do not violate Bowman's membrane or epithelium anteriorly (except at the initial entry point of the incision) nor violate Descemet's membrane posteriorly.

The corneal implant curvature and dimension have been selected according to the nomogram or computer program as described above. The surgeon then inserts or injects the corneal implant into the intrastromal incision all the way to the optical zone mark. It may be necessary to push down on the cornea just anterior to the implant as it is inserted to assist in free passage. The entire implant will rest within the incision such that no portion is exposed. If necessary, a suture may be used to close the initial peripheral incision if gaping occurs. This process is repeated until the desired number of implants have been placed. Fig 5a illustrates an anterior or top view of a cornea containing four radial stromal implants 30. Note that the implants are present within the midperipheral cornea and do not enter the central optical zone or "visual axis," the area immediately surrounding the center of the cornea or corneal apex 32. Note placement of the implants radially with respect to the corneal apex 32 and the corneal periphery or limbus 34. Although this Figure illustrates a symmetric placement of implants, an asymmetric placement may be indicated for correction of astigmatism. One example of this is shown in Fig 5b. In addition, the number of implants to be used may range between 1 to 30, depending upon the type and degree of refractive error to be corrected.

Postoperatively, if residual refractive error is present and it is desirable to correct it, a laser or other heat source can be focused or directed upon the implants within the corneal stroma to effect a change in the implant curvature or dimensions due to heat-shrinkage of the implant material. A suitable laser source would be a typical ophthalmic Argon laser which can be focused to a 50-100 μm spot size and applied accurately to a small portion of the intrastromal implant material. The 488nm or 514nm wavelength of the Argon laser is not absorbed by transparent corneal tissue, but can be selectively absorbed by dyes within the implant material. The amount of change of the curvature or dimensions may be precisely controlled by altering the number of laser applications, the location of laser applications, dye concentration or composition within the implant, the energy per application, the laser spot size, and the laser wavelength. The curvature or length change desired for each intrastromal implant can be determined based upon the corneal curvature immediately surrounding each implant, as can be determined by computerized corneal topography or keratometry. Since heat-shrinkage of the implant material is likely to reduce the conformational change exerted by the implant, it may be desirable to select an initial implant curvature or dimensions which are likely to over-correct the refractive error and then use the laser to accurately reduce the over-correction until the corneal curvature provides the desired refractive error or emmetropia.

Should the implants ever require removal, such as due to selection of incorrect implant dimensions or curvature, a small radial incision may be made in the corneal periphery over the implant material in the

same fashion as described above. The implant material may then be withdrawn with a forceps and the intrastromal incision left empty or a new implant placed within the incision as described above. If the implant material is removed and not replaced, it is expected that the corneal shape and refractive change will be reversible and return to the preoperative state.

Fig 6 illustrates a second embodiment of the apparatus used to facilitate insertion of the intrastromal implants. This embodiment permits simultaneous creation of intrastromal incisions and insertion of intrastromal implants. The apparatus consists of an adapted hypodermic syringe with a narrow tube 40 fitted at one end with a piston 42 and at the other end with a hollow needle 43 and hub assembly 47. An advancing wire 45 extends between the piston 42 and the needle 43. The corneal implant is placed entirely within the bore of the needle 43 between the forward cutting end of the needle and the forward end of the advancing wire 45. This apparatus does not require creation of a separate initial peripheral radial incision. The needle 43 may be curved to facilitate orientation of the needle in the radial direction from corneal periphery to the corneal apex while the syringe 40 is held approximately perpendicular to the corneal limbus. The implant material is preloaded into the bore of the needle in the proper orientation, e.g. curvature up or down. Corneal optical zone markers are used to create marks at the entrance site of the needle in the corneal periphery and at the central optical zone. Radial marks may be made with a conventional radial keratotomy corneal marker to connect the peripheral and central marks. The apparatus is placed with a portion of the needle 43 firmly in contact with the peripheral cornea, limbus, and sclera. The needle 43 is also oriented radially with respect to the center of the cornea and such that the tip enters the cornea at the peripheral corneal mark. The forward cutting end of the needle 43 is then advanced toward the central cornea by the surgeon until reaching the central optical zone mark. The portion of the needle 43 that has not yet entered the corneal stroma remains in contact with the surface of the cornea, limbus, and sclera while the needle 43 is advanced. This serves to stabilize and orient the needle so that it travels within the corneal stroma. The advancing wire 45 is then advanced into the bore of the needle 43 by pushing on the piston 42 in order to push the implant material out of the needle 43 and into the corneal stroma. Advancement of the piston is facilitated by countertraction on the syringe flange 48. Simultaneously, the surgeon removes the needle 43 from the corneal stroma while the implant material is advanced into the stroma, thereby allowing the implant to occupy the potential space created by the needle 43. This allows placement of the implant material within the corneal stroma while minimizing disturbance of surrounding tissue. Alternatively, the implant may be fashioned with a sharpened tip to permit dissection of corneal stroma by advancement of the implant rather than by the needle 43.

While particular embodiments of the invention have been shown and described, it will be obvious to those skilled in the art that changes and modifications may be made without departing from the invention in its broader aspects.

I claim:

1. A method for altering corneal curvature to correct refractive errors, including the steps of:
 - determining pre-existing corneal curvature and refractive error,
 - use of a nomogram or computer program encompassing these variables to determine the required locations, number, depth, and dimensions of corneal implants to correct the refractive error,
 - use of an apparatus to create radial, intrastromal corneal incisions of desired depth and dimensions,
 - insertion of biocompatible implants within said incisions to exert conformational change upon corneal curvature,
 - later modification of the dimensions or curvature of said implants by application of heat from a laser or other means, if required to correct residual refractive error,
 - later modification of dimensions or placement of said implants by removal of implants and replacement by other implants of differing dimensions, if required to correct residual refractive error.
2. The method of claim 1, wherein said incisions are made from the corneal periphery or limbus and extend radially toward the central cornea but do not enter the central visual axis of the cornea.
3. The method of claim 1, wherein said incisions remain within the stroma of the cornea except for the initial entrance at the surface of the cornea.
4. The method of claim 1, wherein said incisions may be created in a two step process whereby a small radial incision is made in the corneal periphery or limbus, followed by a radial incision that begins and continues entirely within the corneal stroma.
5. The method of claim 1, wherein said incisions may be single or a plurality of radial incisions placed symmetrically or asymmetrically to correct particular refractive errors.
6. The method of claim 1, wherein the conformational change exerted upon the cornea from said implants may be changed in-situ by altering the longitudinal or transverse dimensions or curvature of said implants by application of heat from a laser or other source to said implants.
7. The method of claim 1, wherein the conformational change exerted upon the cornea from said implants may be reversed by removal of said implants.
8. The method of claim 1, wherein the conformational change exerted upon the cornea by said implants may be altered by removal of said implants and replacement with said implants of different dimensions.
9. A corneal implant, comprising an elongated body of biocompatible material and curved along the longitudinal dimension.

10. The implant of claim 9, wherein said body of material is composed of polymethylmethacrylate.
11. The implant of claim 9, wherein said body of material is composed of prolene (TM).
12. The implant of claim 9, wherein the longitudinal dimensions may be tapered to facilitate dissection of corneal tissue during insertion.
13. The method of claim 1, wherein said incisions are made by advancing an implant of claim 12 within the corneal stroma.
14. The implant of claim 9, wherein the transverse dimensions may be a plurality of shapes.
15. The implant of claim 9, wherein said body of material is composed of heat-shrinkable plastic.
16. The implant of claim 9, wherein dyes are incorporated within said body of material to allow increased absorption of laser or heat energy by said implant.
17. An apparatus for creation of radial intrastromal incisions extending from the corneal periphery or limbus toward the central cornea, comprising:
 - two handles joined at one end by a spring and at the other end pivoted together
 - a forward end of one of said handles consisting of an angled, narrow, elongated, and tapered member for use in penetrating the corneal surface and dissecting corneal stroma
 - a forward end of the other of said handles consisting of an angled member of sufficient width and length to stabilize said apparatus when placed upon the cornea.
18. An apparatus for creation of radial intrastromal incisions and simultaneous insertion of corneal implants comprising:
 - a syringe consisting of a narrow tube fitted at one end with a piston and at the other end by a hollow needle
 - an advancing wire extending from said piston into said needle
 - an implant of claim 9 present within the bore of said needle between the tip of said needle and said advancing wire within said needle.
19. The apparatus of claim 18, wherein the needle of said apparatus is curved to facilitate insertion and advancement of said needle within the corneal stroma from the corneal periphery or limbus toward the corneal apex.

1/3

FIG. 1

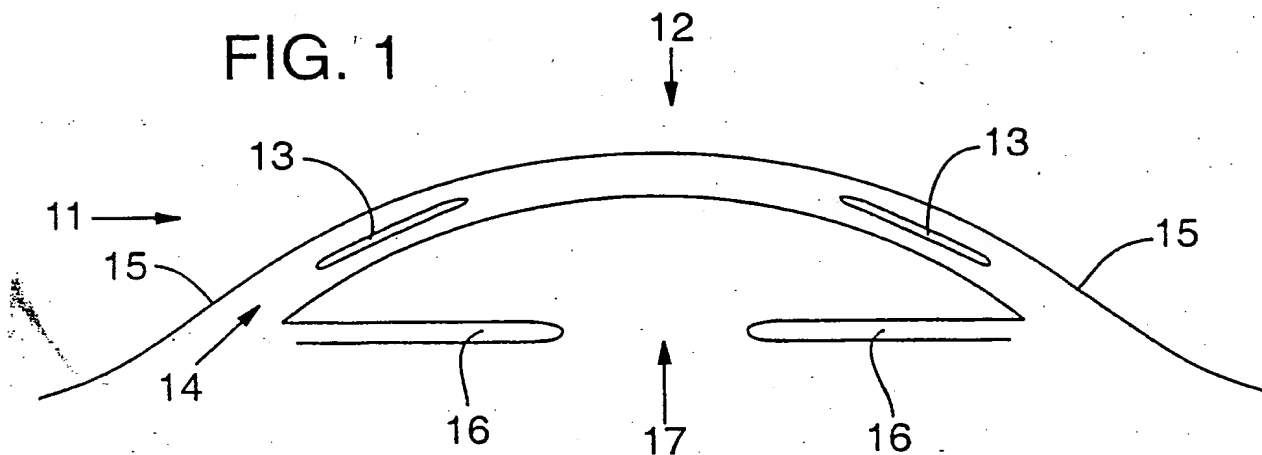


FIG. 2

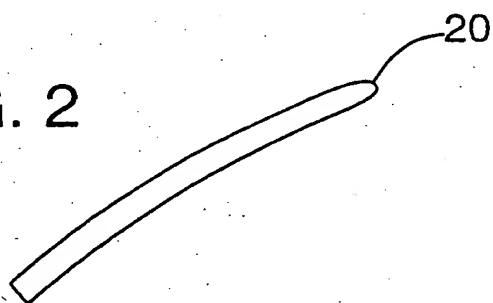
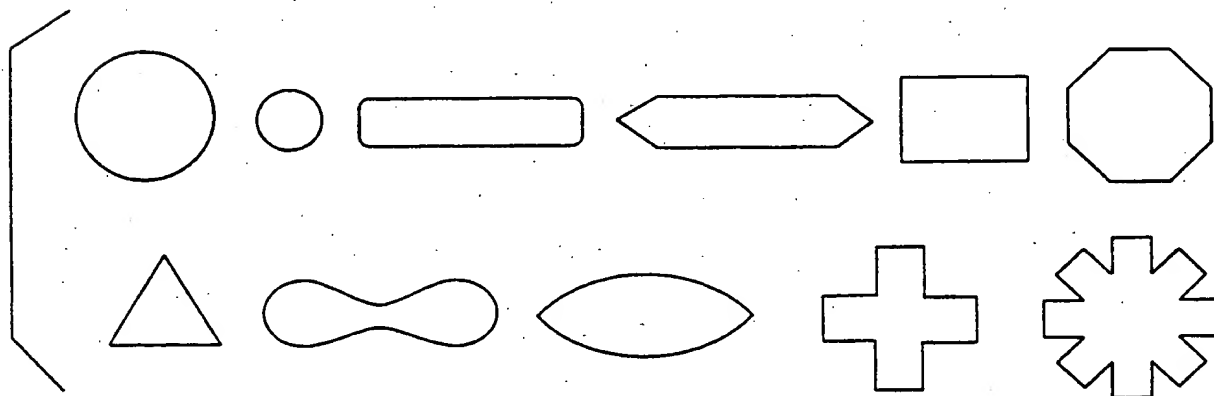
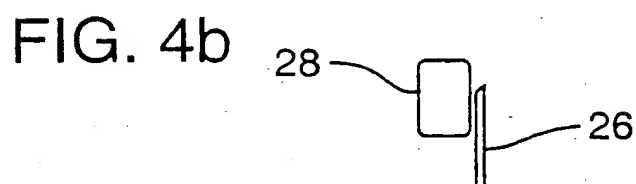
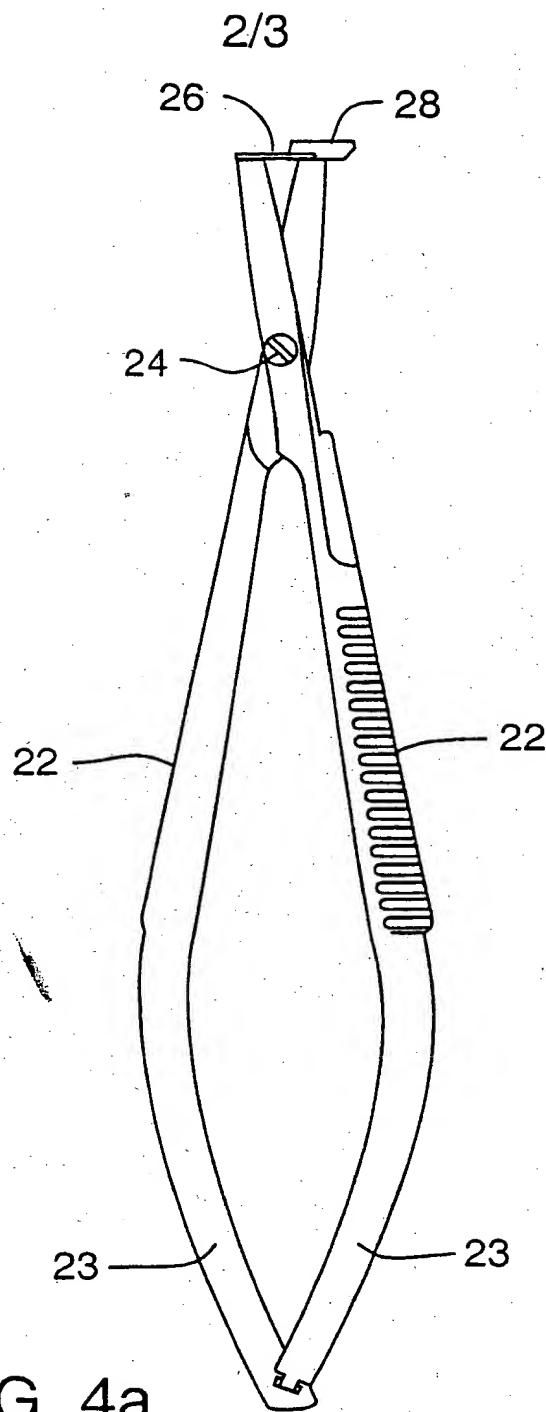


FIG. 3





3/3

FIG. 5a

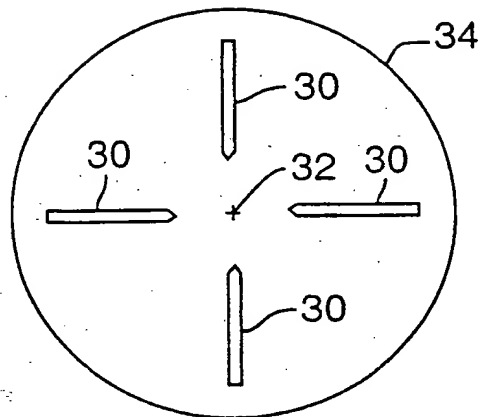


FIG. 5b

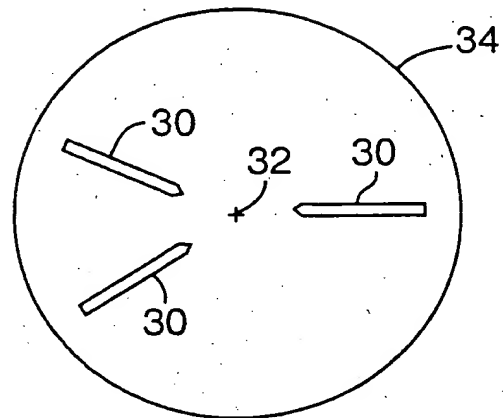
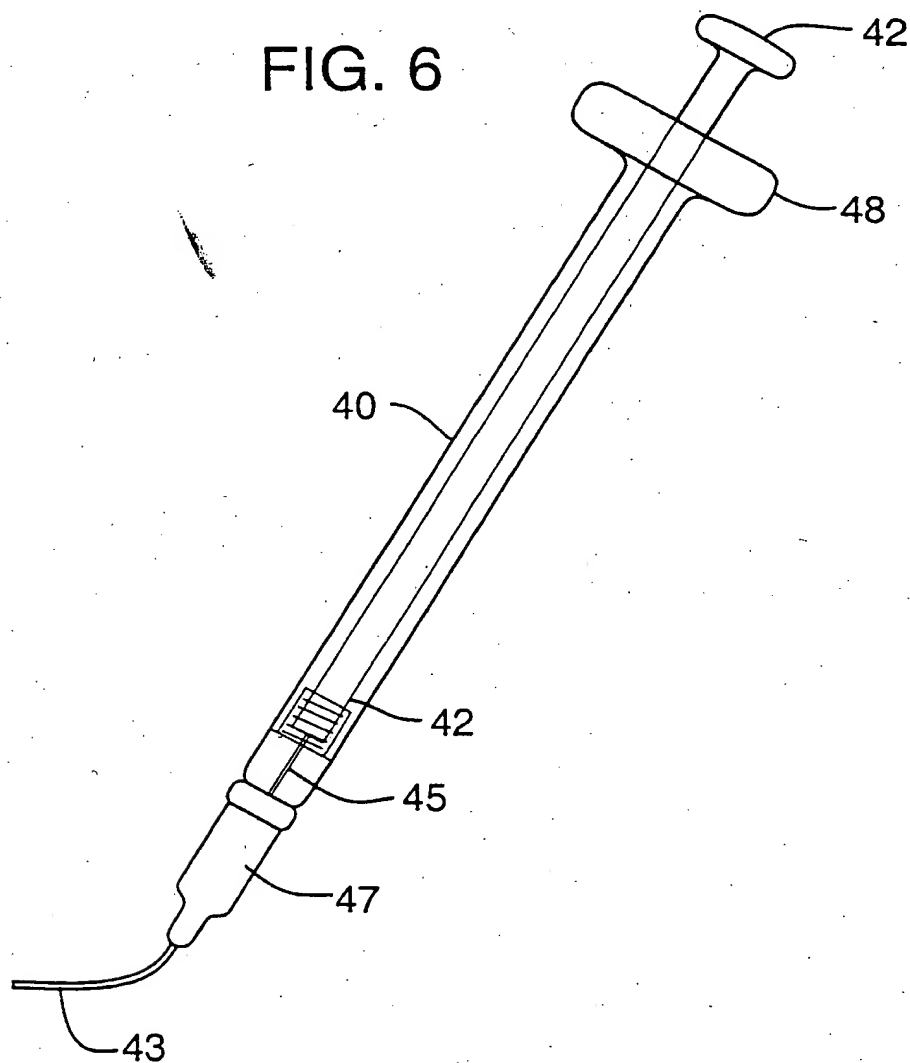


FIG. 6



SUBSTITUTE SHEET (RULE 26)

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US98/05720

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) A61N 5/02

US CL 606/5: 128.898

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. 606/5: 128.898

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y, P	US 5, 722, 971 A (PEYMAN) 03 MARCH 1998, SEE ENTIRE DOCUMENT	1-19
A	US 5, 425, 727 A (KOZIOL) 20 JUNE 1995, SEE ENTIRE DOCUMENT	1-19

☐ Further documents are listed in the continuation of Box C.☐ See patent family annex.

* Special categories of cited documents

A document defining the general state of the art which is not considered to be of particular relevance

E earlier document published on or after the international filing date

L document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

Q document referring to an oral disclosure, use, exhibition or other means

P document published prior to the international filing date but later than the priority date claimed

T

later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

X

document of particular relevance, the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

Y

document of particular relevance, the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

&

document member of the same patent family

Date of the actual completion of the international search

05 JULY 1998

Date of mailing of the international search report

23 JUL 1998

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
Box PCT
Washington, D.C. 20231

Facsimile No. (703) 305-3230

Authorized officer

DAVID J. ISABELLA

Telephone No. (703) 308-3060